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Analysis of deep brain stimulation electrodes: A semi-automatic approach of contact localization

S. Schönfisch^{1,2}, S. Hemm², L. Sarry², M. Saingery², J. Coste^{2, 3}, J. Gabrillargues^{2, 4}, J.J. Lemaire^{2,3} ¹Fachhochschule Oldenburg/Ostfriesland/Wilhelmshaven, Wilhelmshaven, Germany; ²Inserm, ERI 14, Equipe de Recherche en Imagerie Médicale, Clermont-Ferrand, France; ³CHU Clermont-Ferrand, Hôpital Gabriel Montpied, Service de Neurochirurgie A, Clermont-Ferrand, France; ⁴CHU Clermont-Ferrand, Hôpital Gabriel Montpied, Service de Radiologie A, Clermont-Ferrand, France

Introduction

Deep brain stimulation (DBS) has proven to be a highly efficient treatment for Parkinson's disease (PD). By stereotactic surgery, 4contact electrodes (Activa 3389, Medtronic, Minneapolis, USA) can be placed very precisely in the brain. To improve the understanding of the mechanism of action of DBS it is necessary to analyze precisely the anatomical position of each electrode contact and to compare it to the corresponding clinical outcome. Such an analysis necessitates preoperative anatomic images, a postoperative anatomic image series (electrode artifact) and the correspondence between both image series (transformation parameters). We propose in this study a tool able to **semi-automatically identify contact positions on preoperative CT or MR images** and their **projection on the preoperative image** for detailed anatomic analysis. The results obtained with this method were compared to those obtained by manual identification for eight patients.

Image data

Inserm

Materials and Methods

Preoperative stereotactic MRI (Siemens)

•White Matter Attenuated Inversion Recovery (WAIR) T2-weighted sequence
•TR: 4500 msec; TE: 13 msec; Voxel size: 0.52×0.52×2.00 mm³



Figure 1: Identification of the final electrode contact positions via the CT artefact

a) Manual electrode identification

 Merging of preoperative MR images and postoperative CT scan (iPlan, Brainlab, Munich) – mutual information algorithm

Postoperative CT (GE)

- Artifact analysis on the CT scan using the stereotactic planning software (iPlan, Brainlab, Munich) (Figure 1)
 - Middle of artifact in axial direction = electrode
 - Lateral black artifacts = beginning and end of the electrode
 - Deduction of the four electrode contacts and their centers on the CT image
- Extraction of the MR image coordinates (possible due to image fusion) of the contact centers via a neuronavigational software (VVLink, Brainlab, Munich)

b) Semi-automatic electrode identification



•rotation time of 1s, tube voltage 140 kV, effective mAs of 280

•isotropic voxel size after axial reconstruction of 0.43×0.43×0.43 mm³



Two routines were developed (Borland C++ Builder) to semiautomatically identify the electrode contacts based on the homemade software ImageLib:

- 1) indication of the tip and the direction of the electrode in the postoperative image (Figure 2a) by the user
 - calculation of the contact position in image coordinates by the software (Figure 2b,c)
 - → minimization of the squared difference between the expected intensity in artifact center and the voxel intensities
 - → electrode contacts sampled in radial way (tricubic interpolation to obtain sub-voxel accuracy)
- 2) extraction of the transformation parameters between both image series given by the iPlan software
 - calculation of the corresponding MR image coordinates and visualization of the determined contacts (center) on the preoperative image (Figure 2d)

image (Figure 2d) c) Comparison of results obtained with both methods for eight Parkinson patients treated by DBS



Figure 2: Semi-automatic electrode contact identification and visualisation on preoperative images

p' = Rp + t

contact coordinates

•R = Rotation

•p =electrode

•T = Translation



Premier contact x = 219.235 y = 250.700 z = 144.216Second contact x = 221.933 y = 252.356 z = 143.948 Troisième contact x = 224.631 y = 254.012 z = 143.679 Quatrième contact x = 227.328 y = 255.668 z = 143.411

Feasibility for all eight patients Difference between results obtained with both methods are low Mean values < pixel size/ slice thickness (Table 1) Semi-automatic detection = simple to apply;

Manual detection = specialist necessary

mm Δx Δy Δz Mean \pm SD 0.31 ± 0.19 0.14 ± 0.13 0.44 ± 0.36 Min/ Max0.01/0.690.01/0.500.01/1.23

 Table 1: Differences between manually and semi-automatically identified contact coordinates in x, y and z-direction

Discussion

Results

Results show a low mean error compared to slice thickness and pixel size of MR and CT images. The maximal error in the zdirection of 1.23 mm could be due to uncertainties at several levels. In conclusion, we can say that our automatic tool makes the contact localization more objective. Its application can be enlarged to postoperative MR images and to other diseases treated by electrical stimulation. In the future, it should be envisaged to visualize the contact in its dimension on the preoperative MR images (1.5mm height, 1.3mm diameter) in order to further increase the precision of the anatomic position analysis.